

Approximations of the Target-Mediated Drug Disposition (TMDD) Equations for Systems with 1:2 and 2:1 Drug-Target Binding Stoichiometry



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PAGE 2015, June 2-5, Hersonissos, Crete, Greece

Background: TMDD equations were initially written and are used assuming 1:1 stoichiometry of drug-target binding even though many biological systems do not conform to this assumption. Specifically, this assumption is violated for monoclonal antibodies that have two identical binding sites. Although standard TMDD equations provide excellent fit of the observed data, it is of interest to derive correct equations and approximations that assume true binding stoichiometry between the drug and the target.

Objectives: To derive the TMDD model and its approximations for biological systems with 2:1 and 1:2 stoichiometry of drug-target binding.

Methods/Results: TMDD equations for the systems with 2:1 and 1:2 drug target binding were formulated. Quasi-steady state (QSS) assumptions were applied to derive QSS approximations of these systems. QSS systems with zero internalization rate ($k_{int}=0$) or zero dissociation rate ($k_{off}=0$) correspond to quasi-equilibrium (QE) or irreversible binding (IB) approximations of the TMDD equations. Michaelis-Menten (MM) approximations were derived assuming that concentrations of the drug-target complexes are much smaller than concentrations of the free drug.

Conclusions: QSS, QE, IB, and MM approximations of the TMDD models with 1:2 and 2:1 binding were derived. They can be used to provide a more detailed and precise description of the TMDD systems with 1:2 and 2:1 binding stoichiometry than those of the standard TMDD model.

Drug has 2 binding sites; target has 1 binding site:

$$\begin{aligned} \frac{dA_d}{dt} &= -k_a A_d; & A_d(0) &= D_1; \\ \frac{dC}{dt} &= \frac{\ln(t) + F_{SC} k_a A_d + k_{ip} A_T}{V_c} - (k_{el} + k_{pt}) C \\ &\quad - 2k_{on} C \cdot R + k_{off} RC; & C(0) &= D_2 / V_c; \\ \frac{dA_T}{dt} &= k_{pt} C \cdot V_c - k_{ip} A_T; & A_T(0) &= 0; \\ \frac{dR}{dt} &= k_{syn} - k_{deg} R - 2k_{on} C \cdot R + 2k_{off} RC \\ &\quad - k_{on} RC \cdot R + k_{off} RC; & R(0) &= k_{syn} / k_{deg}; \\ \frac{dRC}{dt} &= 2k_{on} C \cdot R - (k_{int} + k_{off}) RC - k_{on} R \cdot RC + 2k_{off} RC; \\ \frac{dR_2C}{dt} &= k_{on} R \cdot RC - (k_{int} + 2k_{off}) R_2C; & R_2C(0) &= R_2C(0) = 0. \end{aligned}$$

Full model: C, R, RC, and R_2C are concentrations of free (unbound) drug, target, and drug complexes with one or two target molecules; k_{el} is linear elimination rate constant, k_{pt} and k_{ip} are inter-compartment rate constants, k_{on} , k_{off} , and k_{int} are binding, dissociation, and internalization (elimination of the complex) rate constants; k_{deg} and k_{syn} are degradation (elimination of the target) and target production rate constants; V_c is central volume; $\ln(t)$ is the infusion rate; F_{SC} is absolute subcutaneous bioavailability. $K_D = k_{off}/k_{on}$; $K_{IB} = k_{int}/k_{on}$

QSS assumptions: $2k_{on} C \cdot R - (k_{int} + k_{off}) RC - k_{on} R \cdot RC + 2k_{off} R_2C = 0$;
 $k_{on} R \cdot RC - (k_{int} + 2k_{off}) R_2C = 0$.
Equivalent to: $2 \cdot C \cdot R = (K_D + K_{IB}) RC + K_{IB} R_2C$;
 $R \cdot RC = (2K_D + K_{IB}) R_2C$

Defining C_{tot} and R_{tot} as $C_{tot} = R + RC + R_2C$ $R_{tot} = R + RC + 2R_2C$
results in: $C = C_{tot} \frac{(K_D + K_{IB})(K_D + K_{IB}/2) + K_{IB} R/2}{(K_D + K_{IB} + R)(K_D + K_{IB}/2 + R)}$;
 $RC = C_{tot} \frac{R(2K_D + K_{IB})}{(K_D + K_{IB} + R)(K_D + K_{IB}/2 + R)}$;
 $R_2C = C_{tot} \frac{R^2}{(K_D + K_{IB} + R)(K_D + K_{IB}/2 + R)}$

$$R = \frac{1}{2} \left[-(2C_{tot} + K_D + K_{IB} - R_{tot}) + \sqrt{(2C_{tot} + K_D + K_{IB} - R_{tot})^2 + 4(K_D + K_{IB})R_{tot}} \right]$$

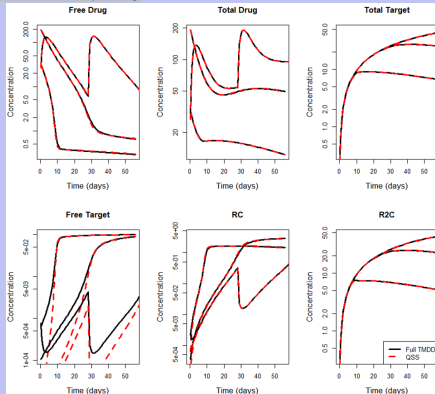
QSS approximation

$$\begin{aligned} \frac{dA_d}{dt} &= -k_a A_d; \\ \frac{dC_{tot}}{dt} &= \frac{\ln(t) + F_{SC} k_a A_d + k_{ip} A_T}{V_c} - (k_{el} + k_{pt}) C_{tot} \\ &\quad - k_{int} C_{tot} \frac{R \cdot (2K_D + K_{IB} + R)}{(K_D + K_{IB} + R)(K_D + K_{IB}/2 + R)}; \\ \frac{dA_T}{dt} &= k_{pt} C \cdot V_c - k_{ip} A_T; \\ \frac{dR_{tot}}{dt} &= k_{syn} - k_{deg} R_{tot} - (k_{int} - k_{deg}) \cdot C_{tot} \cdot \frac{2R}{K_D + K_{IB} + R}; \end{aligned}$$

MM approximation:

$$\begin{aligned} \frac{dA_d}{dt} &= -k_a A_d; \\ \frac{dC}{dt} &= \frac{\ln(t) + F_{SC} k_a A_d + k_{ip} A_T}{V_c} - (k_{el} + k_{pt}) C \\ &\quad - k_{int} \frac{R_{tot} \cdot C}{(K_D + K_{IB})/2 + C}; \\ \frac{dA_T}{dt} &= k_{pt} C \cdot V_c - k_{ip} A_T; \\ \frac{dR_{tot}}{dt} &= k_{syn} - k_{deg} R_{tot} - (k_{int} - k_{deg}) \cdot \frac{R_{tot} \cdot C}{(K_D + K_{IB})/2 + C}; \end{aligned}$$

Simulations: Concentration-time profiles from the full TMDD model and the corresponding QSS approximation were simulated for 3 dosing regimens: 100 mg IV, 600 mg IV, and 100 mg SC (2 doses). $CL=0.3$; $V_c=3$; $V_p=3$; $Q=0.2$; $k_i=0.5$; $F_{SC}=0.7$; $k_{on}=25$; $k_{off}=1$; $k_{int}=0.01$; $k_{syn}=1$; $k_{deg}=10$. Simulations demonstrated a good agreement between exact and approximate equations, except for free target at very low concentrations. Additional investigations are planned to investigate applicability of this approximation across the range of system parameters.



Drug has 1 binding sites; target has 2 binding sites:

$$\begin{aligned} \frac{dA_d}{dt} &= -k_a A_d; & A_d(0) &= D_1; \\ \frac{dC}{dt} &= \frac{\ln(t) + F_{SC} k_a A_d + k_{ip} A_T}{V_c} - (k_{el} + k_{pt}) C \\ &\quad - 2k_{on} C \cdot R + k_{off} RC - k_{on} C \cdot RC + 2k_{off} R_2C; & C(0) &= D_2 / V_c; \\ \frac{dA_T}{dt} &= k_{pt} C \cdot V_c - k_{ip} A_T; & A_T(0) &= 0; \\ \frac{dR}{dt} &= k_{syn} - k_{deg} R - 2k_{on} C \cdot R + k_{off} RC; & R(0) &= k_{syn} / k_{deg}; \\ \frac{dRC}{dt} &= 2k_{on} C \cdot R - (k_{int} + k_{off}) RC - k_{on} C \cdot RC + 2k_{off} R_2C; \\ \frac{dR_2C}{dt} &= k_{on} C \cdot RC - (k_{int} + 2k_{off}) R_2C; & R_2C(0) &= R_2C(0) = 0. \end{aligned}$$

Full model: C, R, RC, and R_2C are concentrations of free (unbound) drug, target, and target complexes with one or two drug molecules; k_{el} is linear elimination rate constant, k_{pt} and k_{ip} are inter-compartment rate constants, k_{on} , k_{off} , and k_{int} are binding, dissociation, and internalization (elimination of the complex) rate constants; k_{deg} and k_{syn} are degradation (elimination of the target) and target production rate constants; V_c is central volume; $\ln(t)$ is the infusion rate; F_{SC} is absolute subcutaneous bioavailability. $K_D = k_{off}/k_{on}$; $K_{IB} = k_{int}/k_{on}$

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 $k_{on} C \cdot RC - (k_{int} + 2k_{off}) R_2C = 0$.
Equivalent to: $C \cdot R = (K_D + K_{IB}) RC / 2 + K_{IB} R_2C / 2$;
 $C \cdot RC = (2K_D + K_{IB}) R_2C$.

Defining R_{tot} and C_{tot} as $R_{tot} = R + RC + R_2C$ $C_{tot} = C + RC + 2R_2C$
results in: $R = R_{tot} \frac{(K_D + K_{IB})(K_D + K_{IB}/2) + K_{IB} C/2}{(K_D + K_{IB} + C)(K_D + K_{IB}/2 + C)}$;
 $RC = R_{tot} \frac{C(2K_D + K_{IB})}{(K_D + K_{IB} + C)(K_D + K_{IB}/2 + C)}$;
 $R_2C = R_{tot} \frac{C^2}{(K_D + K_{IB} + C)(K_D + K_{IB}/2 + C)}$

$$C = \frac{1}{2} \left[(C_{tot} - 2R_{tot} - K_D - K_{IB}) + \sqrt{(C_{tot} - 2R_{tot} - K_D - K_{IB})^2 + 4(K_D + K_{IB})C_{tot}} \right]$$

QSS approximation (MM approximation is obvious, $C_{tot} = C$, and not shown)

$$\begin{aligned} \frac{dA_d}{dt} &= -k_a A_d; \\ \frac{dC_{tot}}{dt} &= \frac{\ln(t) + F_{SC} k_a A_d + k_{ip} A_T}{V_c} - (k_{el} + k_{pt}) C_{tot} - k_{int} \frac{2R_{tot} C}{K_D + K_{IB} + C}; \\ \frac{dA_T}{dt} &= k_{pt} C \cdot V_c - k_{ip} A_T; \\ \frac{dR_{tot}}{dt} &= k_{syn} - k_{deg} R_{tot} - (k_{int} - k_{deg}) \cdot R_{tot} \cdot \frac{C \cdot (2K_D + K_{IB} + C)}{(K_D + K_{IB} + C)(K_D + K_{IB}/2 + C)}; \end{aligned}$$

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