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# Overview of absorption models and modelling issues

Mats O. Karlsson and Rada Savic

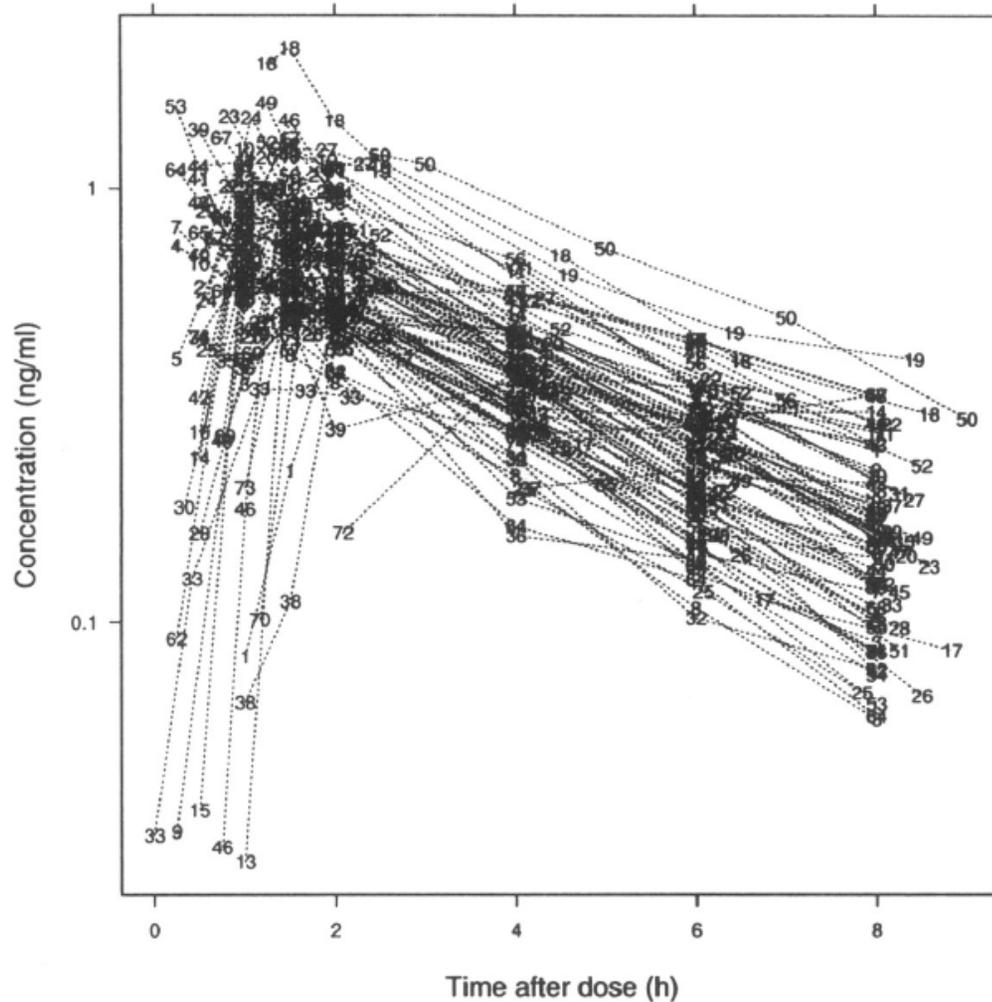
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Uppsala University*



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# Modelling oral absorption

**"Representative" pop PK data set** **Representative absorption modelling**



"Exposure"  $\Rightarrow$  Sparse  
main interest absorption data

Sparse data  $\Rightarrow$  Simple model



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# Outline

- Extent of absorption
- Absorption delay
- Rate of absorption



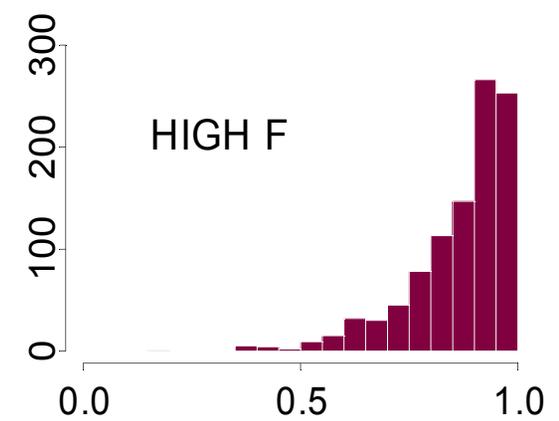
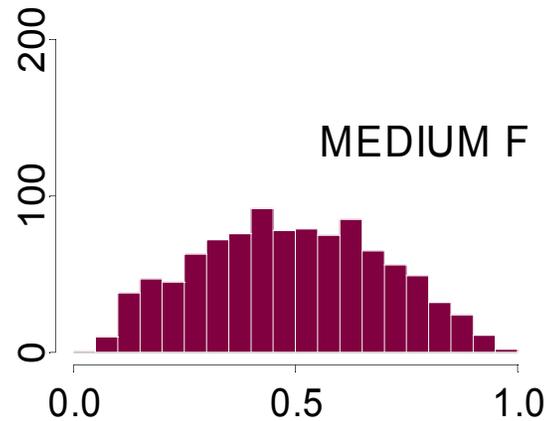
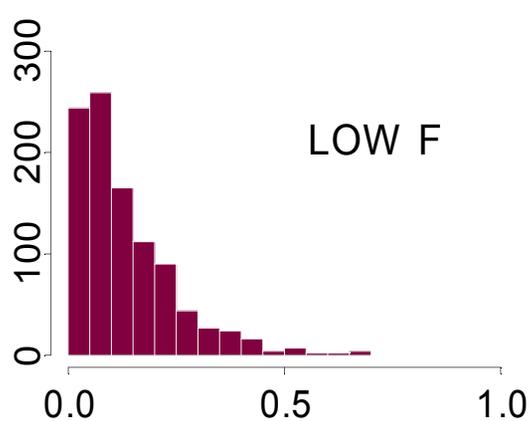
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# Extent (F) – with iv reference dose

$$0 \leq F \leq 1$$

$$F = \frac{e^{\theta+\eta}}{1 + e^{\theta+\eta}}$$

$$F = \frac{e^{\ln(\theta/(1-\theta))+\eta}}{1 + e^{\ln(\theta/(1-\theta))+\eta}}$$





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## Extent (F) – with iv reference dose

### What if (apparently) $F > 1$ ?

Nonlinear disposition

→ Model it!

IOV in CL

→ Model it!<sup>1</sup>

Variability in content amount

→ Model it?\*

Study conduct errors

→ Investigate it!

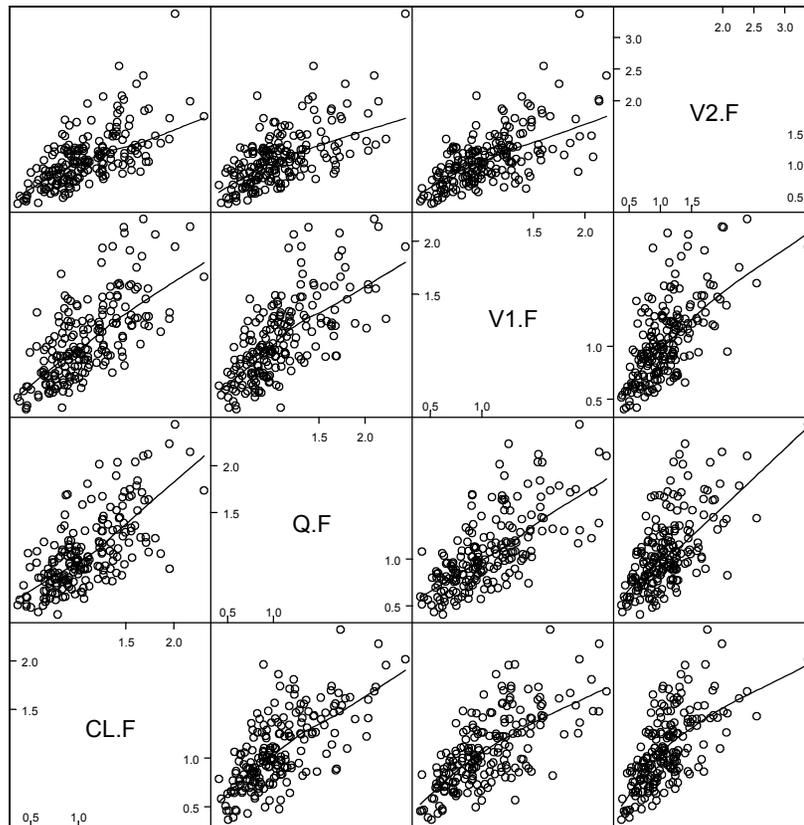
$$* F = \frac{e^{\theta+\eta}}{1 + e^{\theta+\eta}} + \eta_{FORM} \quad \text{With } \eta_{FORM} \text{ fixed to known variability}$$

<sup>1</sup>Karlsson & Sheiner. CPT 1994, 55:623-37



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# Extent (F) – no reference dose



Lack of reference dose  $\longrightarrow$  Parametrisation  
CL/F, Q/F, V1/F, ...

Variability in F  $\longrightarrow$  Parameter correlation

Parameter correlation  $\longrightarrow$  Estimate all (6) covariances

$\longrightarrow$  Estimate variability in "F"

$$F = e^{\eta_F}$$

- 1 instead of 6 parameters (maybe)
- $\eta_F$  for diagnostic purposes
- Caution in interpretation:  $\eta_F$  may reflect other sources of positive parameter correlation (free fraction, body size, ...)

# First-pass effect –

Variability in  $E_H$  will influence both  $CL_H$  and  $F_H$

## Solution 1

Model fixed effects as influencing CL and F separately

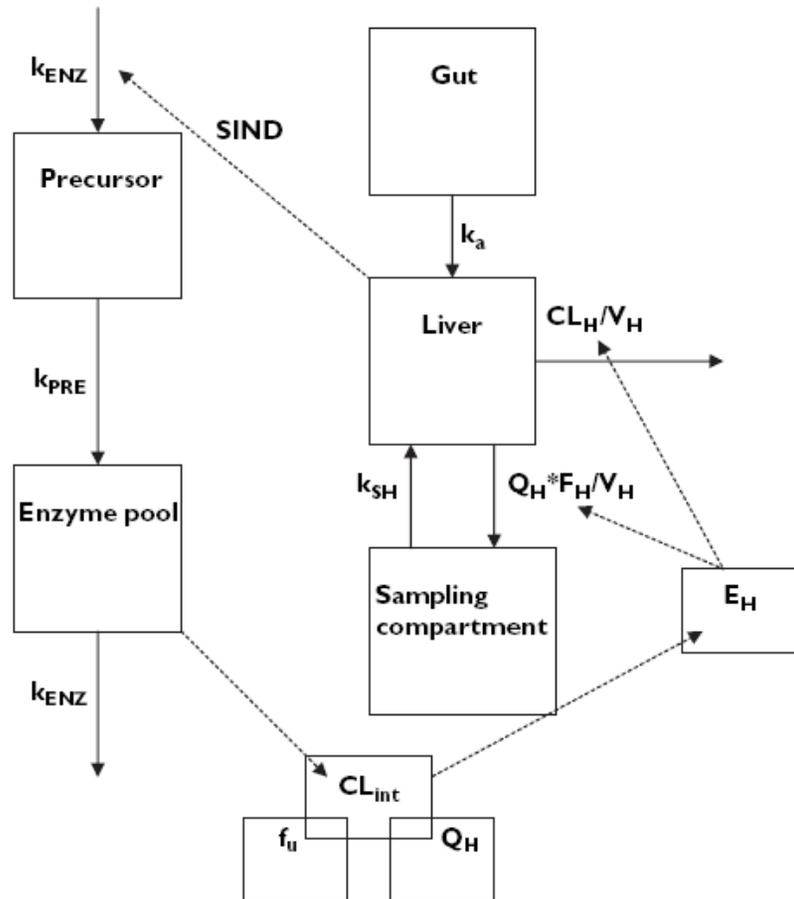
Use a (negative) correlation between CL and F

Unnecessarily many parameters!

## Solution 2

Create a semiphysiological model where covariate influences and variability can be associated with the single appropriate process

# "Mechanistic" modelling of $CL_H$ & $F_H$



⇒ Covariate effect in 1 place only

⇒ Variability in  $CL_{int}$  affects both  $CL_H$  &  $F_H$

⇒ Drug in absorption phase contributes to event in liver



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# Absorption delay modelling

1. Lag time
2. Erlang-type absorption  
*(hard-coded transit compartments)*
3. Transit compartment model  
*(flexible number of transit compartments)*



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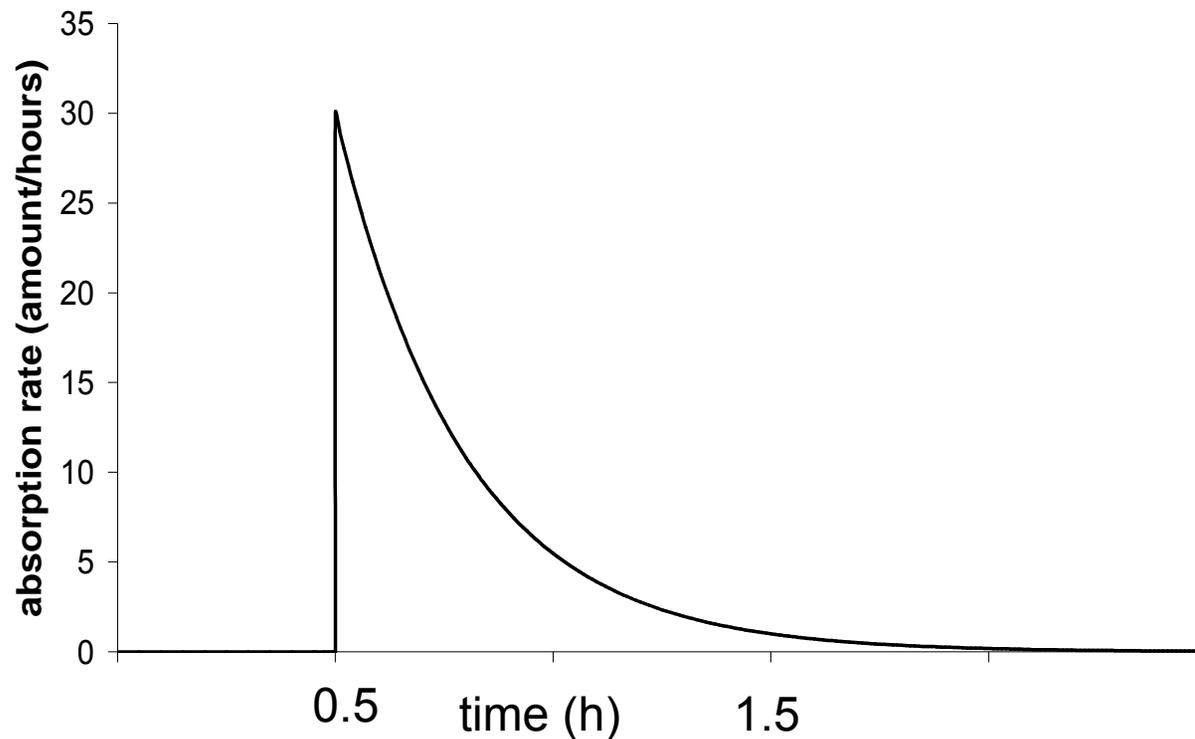
# Lag time model

Often used

It improves the model fit

Unphysiological

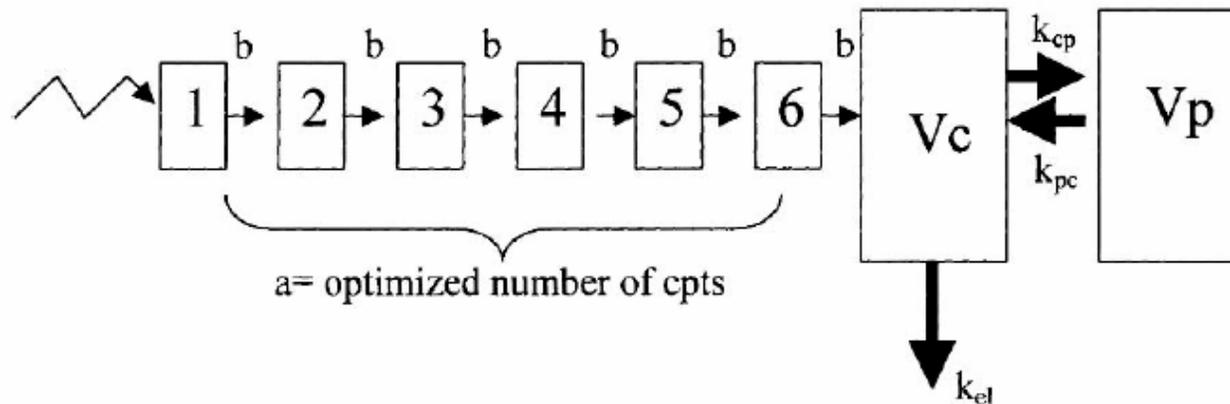
Change-point model (*numerical difficulties esp. with FOCE*)





# Erlang type absorption

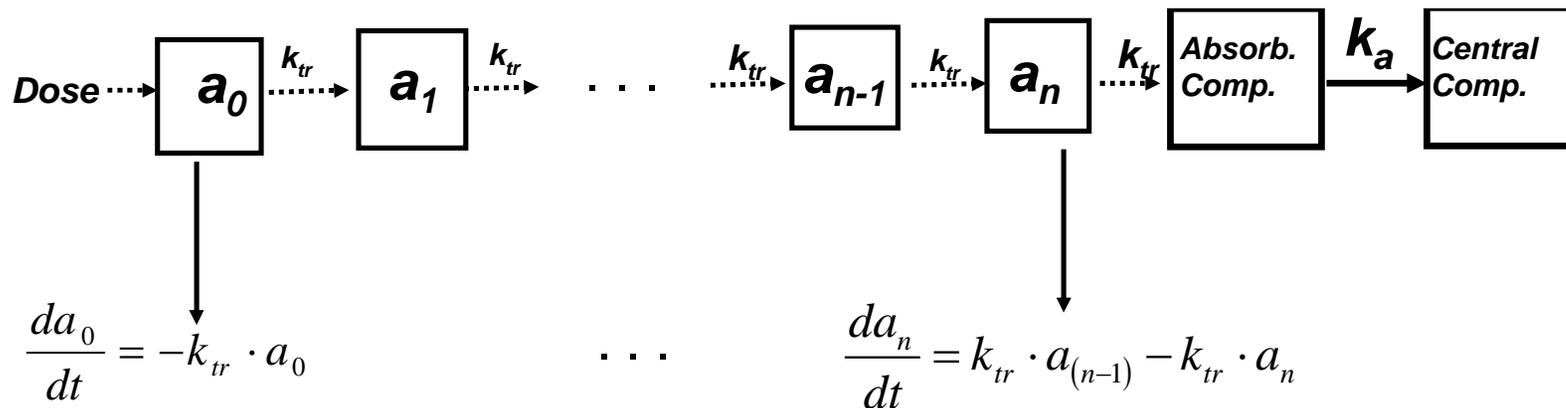
- ✓ Characterises the skewed and delayed absorption profiles
- ✓ Not a change point model
- ✓ No of transit compartments has to be optimised manually
- ✓ Does not have an absorption compartment





# Transit compartment model

- ✓ No of transit compartments (along with variability) is estimated
- ✓ Equivalent to a gamma distribution function
- ✓ Not a change-point model
- ✓ General model (previous two models special cases of this model)





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# Complexity of the absorption process

- Delayed or incomplete gastric emptying
- Changes along the GI tract
  - Absorptive area, motility/mixing, pH, gut wall properties (metabolic enzymes, transporters), content properties, ...
- Competing processes for drug disappearance
- Nonlinearities
  - High local concentrations may lead to incomplete solubilisation, saturation of enzymes and transporters
  - Nonlinearities usually modelled as dose-dependent, rather than dependent on local concentration
- "Discrete" events
  - Gastric emptying, disintegration, food, bile release, absorption windows, motility
- Drug-drug interactions
- Formulation



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# Rate of absorption

## Typical absorption models

✓ First order model

✓ Zero order model

## Why successful?

⇒ Lack of data

⇒ Lack of impetus

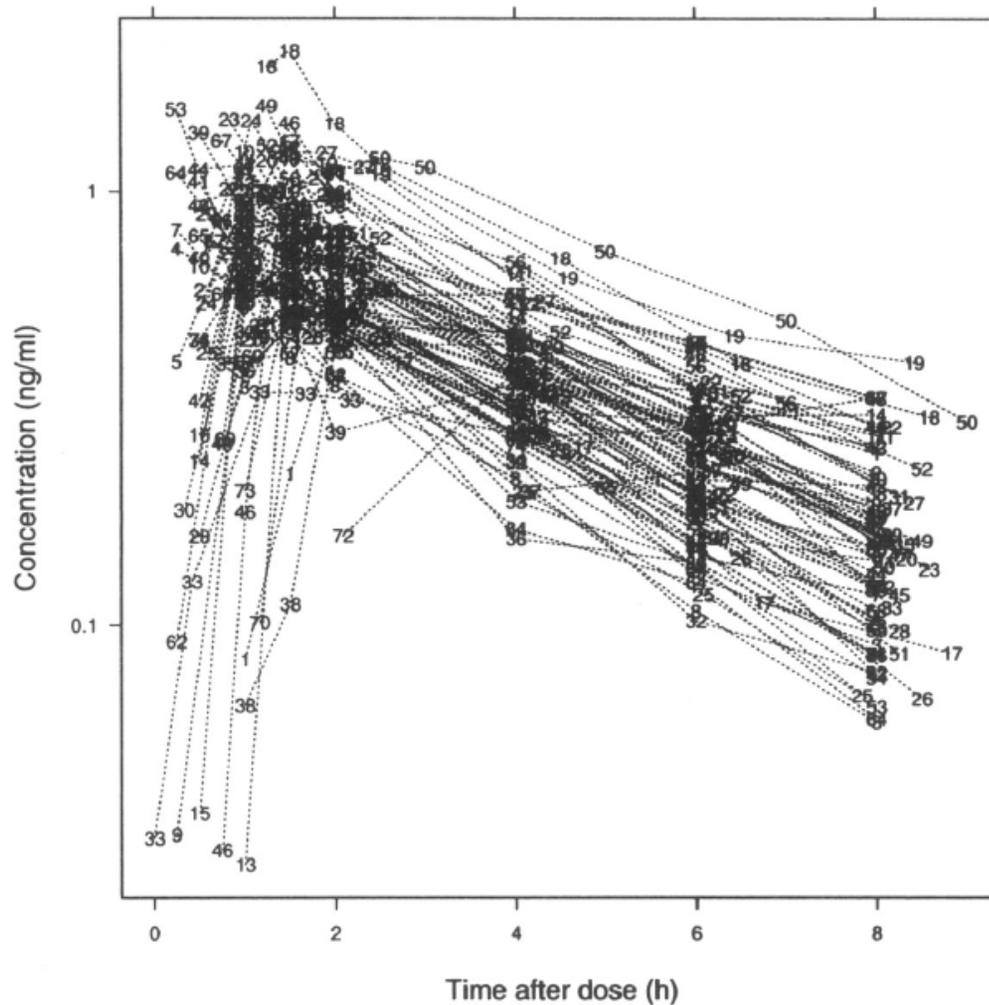
⇒ Lack of models



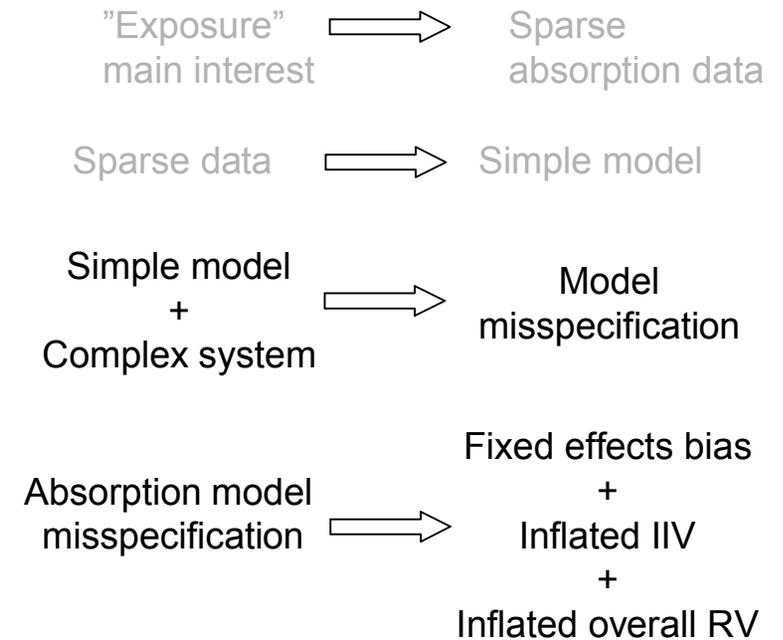
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# Modelling oral absorption

## Representative pop PK data set



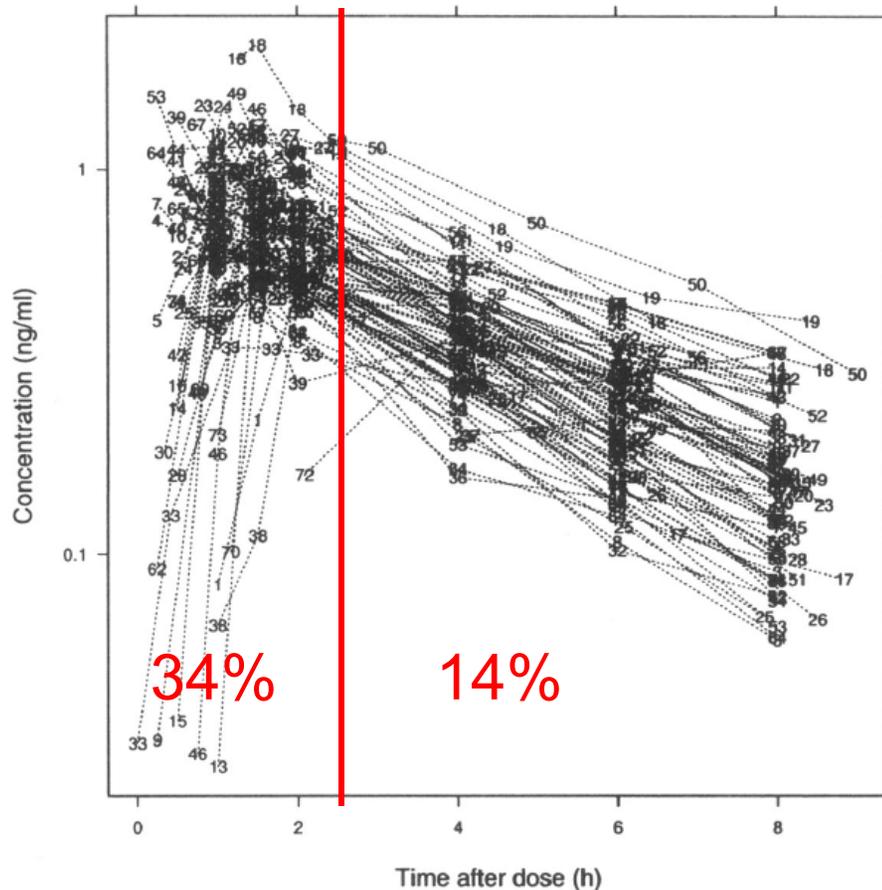
## Representative absorption modelling



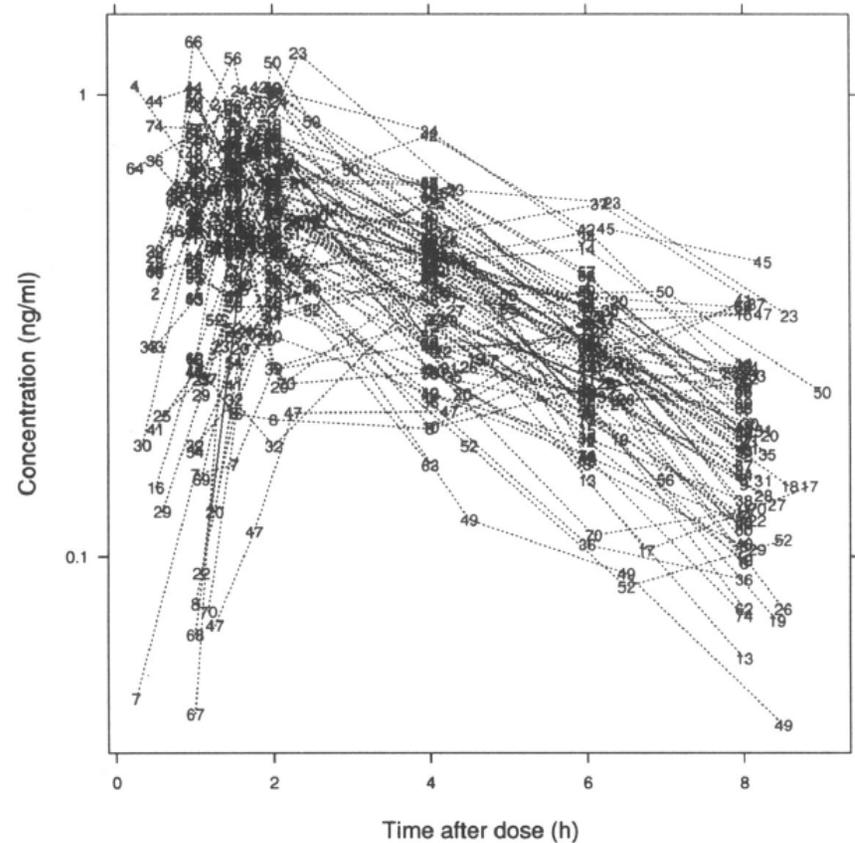


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# Ignoring absorption model misspecification



**Fig. 1.** Observed concentrations after the first dose vs. time after dose plotted on a semilogarithmic scale. Data points are labeled by the ID number and each individual's data points are connected.



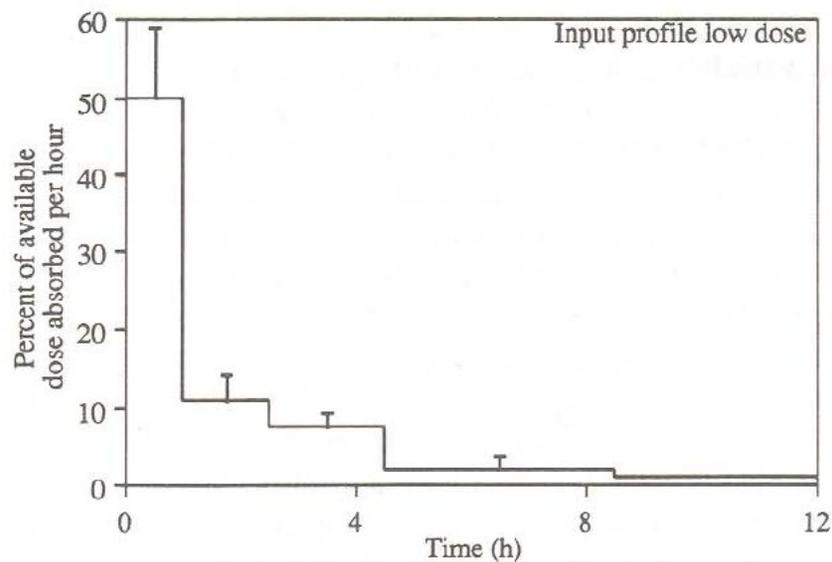
**Fig. 13.** The logarithm of the "observed" simulated concentrations vs. time after dose for one of the simulated data sets. Individual concentrations are connected by broken lines and labeled by ID numbers.



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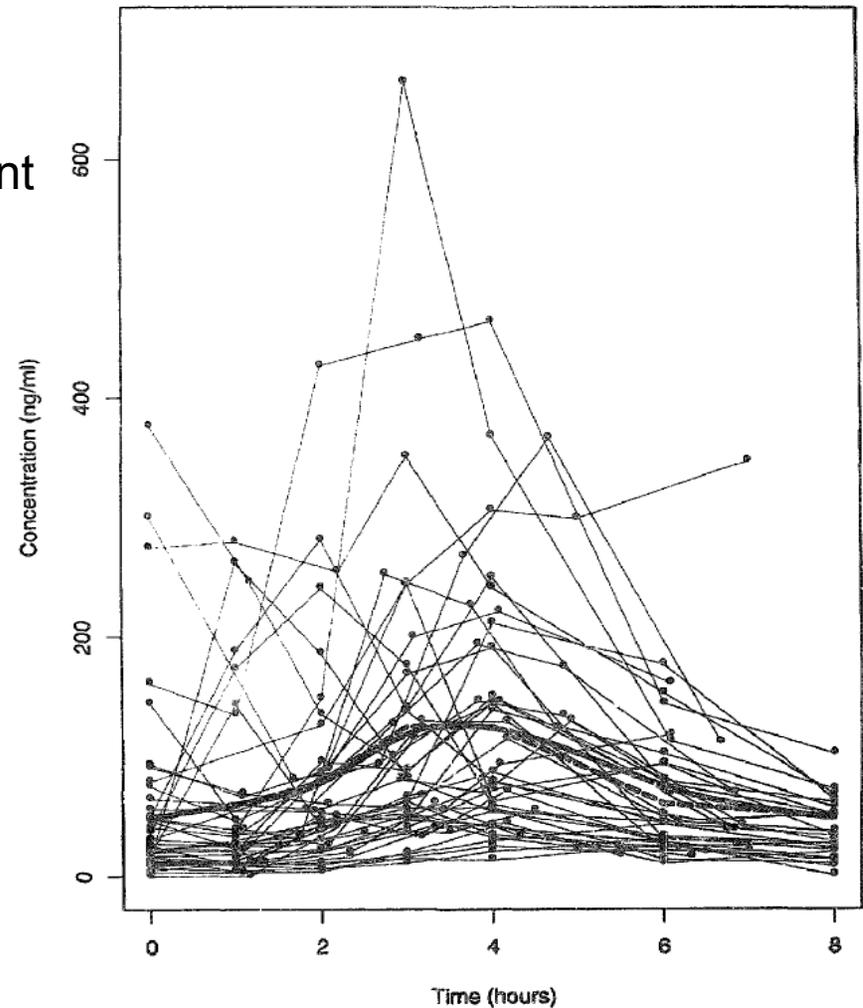
# Flexible absorption models

No estimated change-points  
Easily adapted to information content  
Empirical



*NONMEM code in web-version of presentation*

Lindberg-Freijs et al. Biopharm Drug Disp 1994, 15:75-86



Park et al. JPB 1997, 25:615-48



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# Rate of absorption – other models

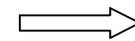
✓ Parallel first order absorption

✓ Mixed zero order and first order  
(simultaneous or sequential)



Used as mechanistic & empirical

✓ Weibull type absorption  
(1 or 2 Weibull functions)



Often overparametrised

✓ Saturable absorption  
(Michaelis-Menten absorption)



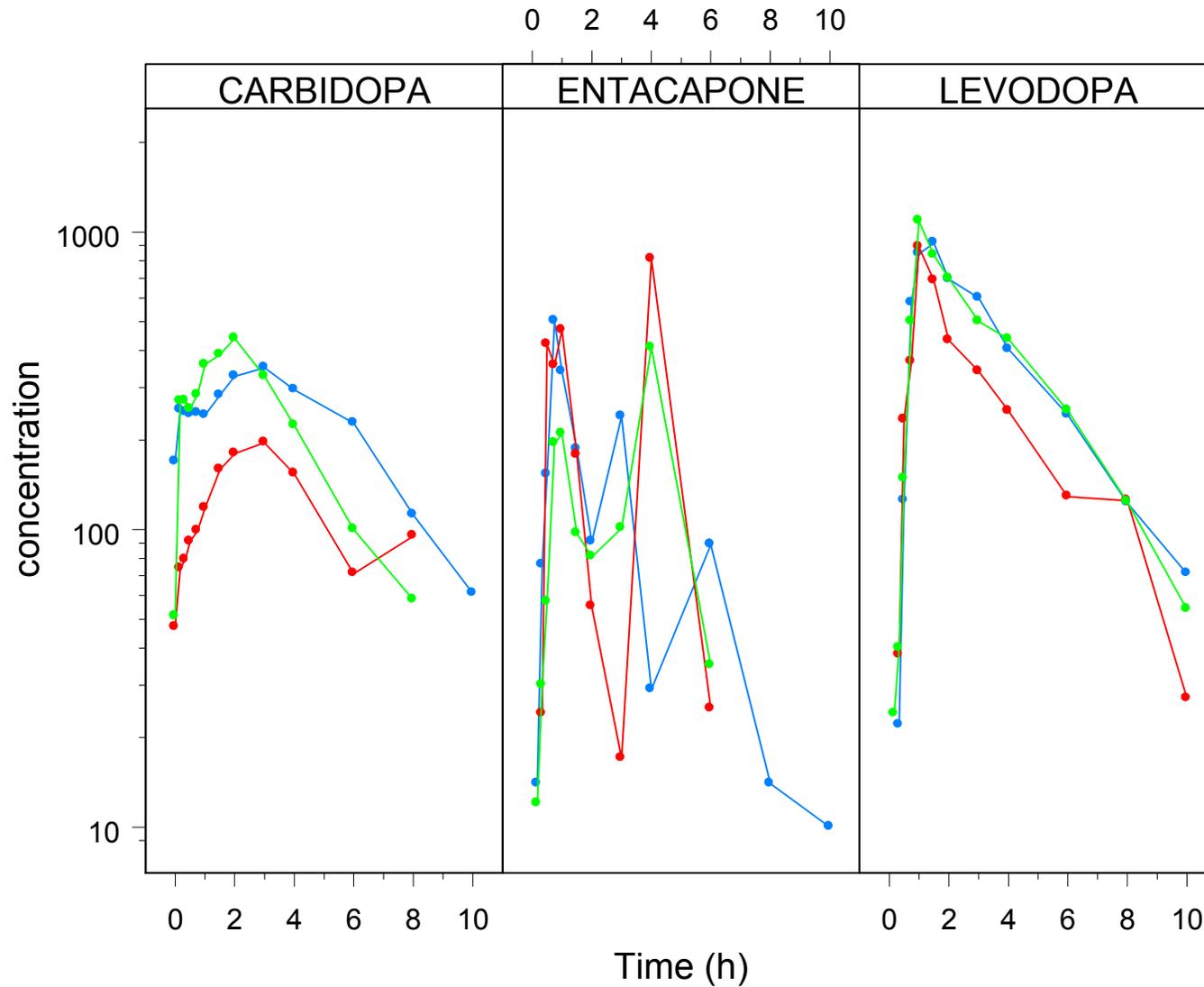
Often change-point models

✓ Inverse Gaussian density absorption

✓ Time-dependent absorption models

Ref in web-version for Holford et al; Higaki et al; Reigner et al., Williams et al.; Zhou; Valenzuela et al.;etc

# Simultaneous dosing of 3 drugs





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# How to model absorption?

## Present modelling approach

Model based on  
(sparse) data only

Prior information  
(essentially) ignored

Model misspecification  
(partially) ignored

## Present simulation approach

Prior information  
(partially) included

Data information used in  
"ad hoc" procedure

## Ideal approach

Posterior model  
obtained as weighted  
balance between prior  
info and data

Study designs adapted  
to information sought



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Extra slides



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# Flexible Input Model

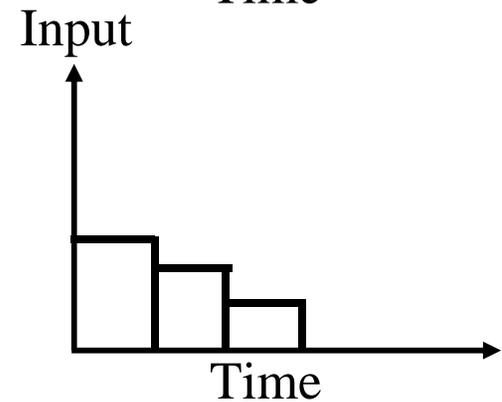
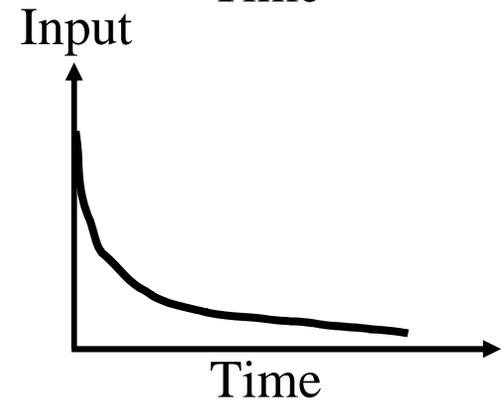
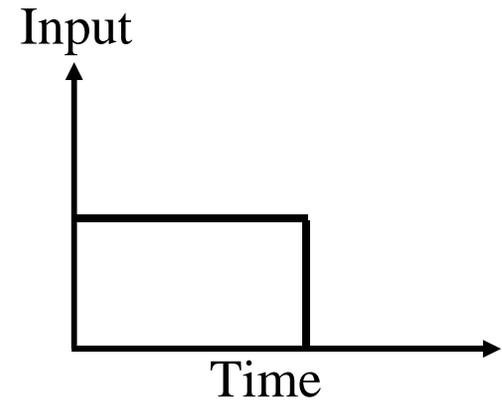
Mats Karlsson, Janet R Wade and Stuart  
Beal

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With a zero-order input, the input rate is constant over time for a finite period.

With a first-order input, the input rate is exponentially decreasing over time.

With the flexible input model, the input rate is an arbitrary step function over a period of time.



# Limitations

The idea applies to a single dose with no other drug on board, for example, a single dose cross-over type study. It can be adapted for some multiple dose situations.

The number of steps needed is fixed and determined by trial and error, using the minimum objective function as a guide. However, this number is limited by the number of observations available during the absorption phase.

The duration of the  $D_i$  of the  $i$ th step is finite and fixed, and is determined by trial and error, shorter durations being tried during the initial part of the absorption phase, when the input rate should be changing most rapidly.

The height  $H_i$  of the  $i$ th step is estimated. It can be expressed as a fraction of the bioavailable dose absorbed over the  $i$ th step per unit time.

# Constraints

One might constrain the heights to be monotonically decreasing, and often they are estimated to be decreasing. However, they may not be decreasing and attention should be paid to this.

The  $H_i$  can be modeled using a number of different  $\eta$ 's. A less flexible model for random interindividual variability can be considered.

In the example IV data are present. If such data are not available bioavailability should be constrained to 1 (and then  $V_d$  is volume relative to true bioavailability).

# Implementation - Data

A *single* dose of 1000 units given at 0 hours.

#ID	TIME	DV	AMT	RATE	EVID	PO
#ORAL DOSE						
1	0	.	1000	-1	1	1
1	0.5	59	.	.	0	1
1	1.0	99	.	.	0	1
1	2.0	90	.	.	0	1
1	3.0	80	.	.	0	1
1	4.0	73	.	.	0	1
1	6.0	55	.	.	0	1
1	8.0	43	.	.	0	1
1	10.	23	.	.	0	1
#IV DOSE						
1	0	.	1000	.	4	0
1	0.5	399	.	.	0	0
1	1.0	191	.	.	0	0
1	2.0	120	.	.	0	0
1	3.0	90	.	.	0	0
1	4.0	69	.	.	0	0
1	6.0	51	.	.	0	0
1	8.0	46	.	.	0	0
1	10.	28	.	.	0	0

# Implementation – Control Stream

```
$INPUT  ID  TIME  DV  AMT  RATE  EVID  PO
$DATA   DATA1  IGNORE #
$SUBROUTINE ADVAN1 TRANS2
$PK
;THETA(1)= CLEARANCE
;THETA(2)= VOLUME
;THETA(3)= BIOAVAILABILITY

IF (TIME.EQ.0) DOSE = AMT

;DISPOSITION AND SCALE MODELS
CL = THETA(1) * EXP(ETA(1))
V  = THETA(2) * EXP(ETA(2))
S1 = V

;BIOAVAILABILITY MODEL
F1 = PO*THETA(3)*EXP(ETA(3))+(1-PO)

;ABSORPTION MODEL
; variables indicating the active step
Q1 = 0
Q2 = 0
Q3 = 0
IF(TIME.LE.1)           Q1 = PO
IF(TIME.GT.1.AND.TIME.LE.3) Q2 = PO
IF(TIME.GT.3.AND.TIME.LE.6) Q3 = PO
```

```

; fraction of bioavailable dose
;   absorbed over step, per unit time
DEN   = 1+THETA(4)*EXP(ETA(4))+ THETA(5)*EXP(ETA(5))
ABR1  = 1/DEN
ABR2  = THETA(4)*EXP(ETA(4))/DEN/2
ABR3  = THETA(5)*EXP(ETA(5))/DEN/3

R1 = F1*DOSE*(Q1*ARB1+Q2*ARB2+Q3*ARB3)

;           CL           V           F           04           05
$THETA  (0,10)  (0,100)  (0,1)  (0,0.4)  (0,0.3)

;           CL           V           F
$OMEGA  .1    .1    .1

$OMEGA  BLOCK(2)  .2  .1  .2

```

# Reference

A Lindberg-Freijs & MO Karlsson.  
Dose dependent absorption and linear  
disposition of cyclosporin A in rat.  
Biopharmaceutics & Drug Disposition  
Vol 15, 75-85 (1994).



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# Transit compartment model

Radojka Savic, Daniel Jonker, Thomas  
Kerbusch and Mats Karlsson

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# Implementation – Control Stream

```
$PROB TRANSIT COMPARTMENT MODEL
$INPUT ID AMT TIME DV CMT EVID
$DATA data1.dta IGNORE=#
$SUBROUTINES ADVAN6 TOL5
$MODEL COMP=(ABS)
        COMP=(CENT)
```

```
$PK
```

```
IF (AMT.GT.0.AND.CMT.EQ.1) PODO=AMT ; oral dosing
IF (AMT.GT.0.AND.CMT.EQ.2) PODO=0  ; intravenous dosing
```

```
;DISPOSITION MODEL
```

```
CL      =THETA(1)*EXP(ETA(1))      ; Clearance
V2      =THETA(2)*EXP(ETA(2))      ; Volume of distribution
```

```
; BIOAVAILABILITY MODEL
```

```
F1      =0
```

```
; The amount is explicitly used in differential equation describing
the absorption process
```

```
F2      =1
```

```
BIO     =THETA(2)*EXP(ETA(2))      ; Bioavailability
```



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; Absorption model

**KA** =**THETA(4)\*EXP(ETA(4))** ; Absorption rate constant  
**MTT** =**THETA(5)\*EXP(ETA(5))** ; Mean transit time  
**N** =**THETA(6)\*EXP(ETA(6))** ; Number of transit compartments  
**KTR** =**(NN+1)/MTT** ; transit rate constant

;NFAC =**SQRT(2\*3.1415)\*NN\*\*(NN+0.5)\*EXP(-NN)**  
; Stirling approximation to n! function

**LNFAC=LOG(2.5066)+(NN+0.5)\*LOG(NN)-NN**  
; Logarithm of Stirling approximation

**\$DES**

;DADT(1)=**BIO\*PODO\*KTR\*(KTR\*T)\*\*NN\*EXP(-KTR\*T)/NFAC-KA\*A(1)**  
; Original equation, might cause some numerical difficulties,  
therefore the log-transformation of original equation is needed

**DADT(1)=EXP(LOG(BIO\*PODO+.00001)+LOG(KTR)+NN\*LOG(KTR\*T+.00001)-**  
**KTR\*T-LNFAC)-KA\*A(1)**

; Log-transformed equation, small number (0.00001) is added to  
avoid Log(0)

**DADT(2)=KA\*A(1)-K\*A(2)**



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## Reference

Radojka M. Savic, Daniël M. Jonker, Thomas Kerbusch &  
Mats O Karlsson

Evaluation of a transit compartment model versus a  
lag time model for describing drug absorption  
delay

PAGE 13 (2004) Abstr 513 [[www.page-meeting.org/?abstract=513](http://www.page-meeting.org/?abstract=513)]